

Symposium on AI and Reconstruction for
Biomedical Imaging, March 9-10, 2026

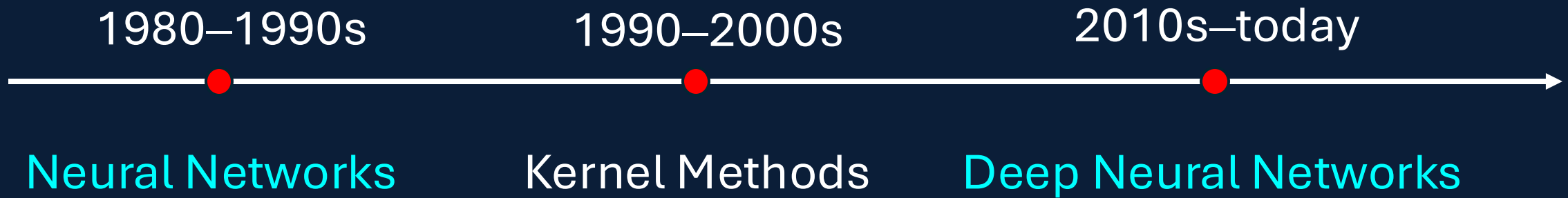
Bridging Physics and Learning: A Decade of Kernel Methods for Image Reconstruction

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Ideas in Machine Learning Come in Cycles



Where do kernel methods fit today?

Image Reconstruction: Physics-based Inverse Problem

- Imaging physics provides a forward model linking the unknown image $\mathbf{x}$ to measured data $\mathbf{y}$

$$y_i \sim \text{Poisson}(\bar{y}_i), \quad \bar{\mathbf{y}} = \mathbf{P}\mathbf{x} + \mathbf{r}$$

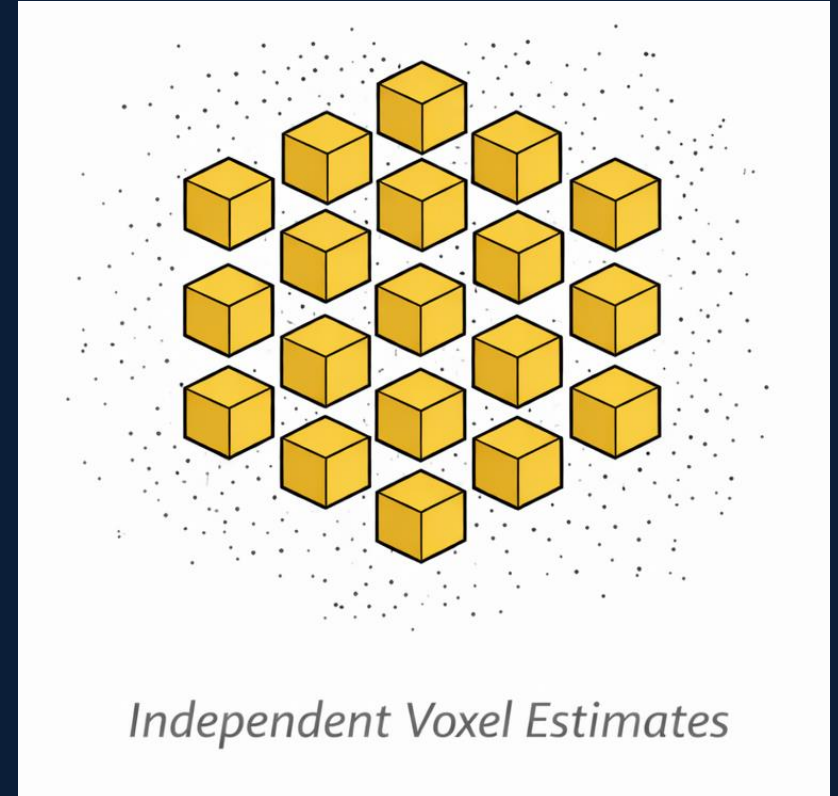
- Classic inverse problem: image reconstruction using the maximum-likelihood estimation

$$\hat{\mathbf{x}} = \arg \max_{\mathbf{x}} L(\mathbf{y} | \mathbf{x})$$

A Geometric Perspective of Image Voxels

Maximum-Likelihood Reconstruction

- Voxels are treated independent
- Image space = Euclidean grid
- Coupling only through imaging physics



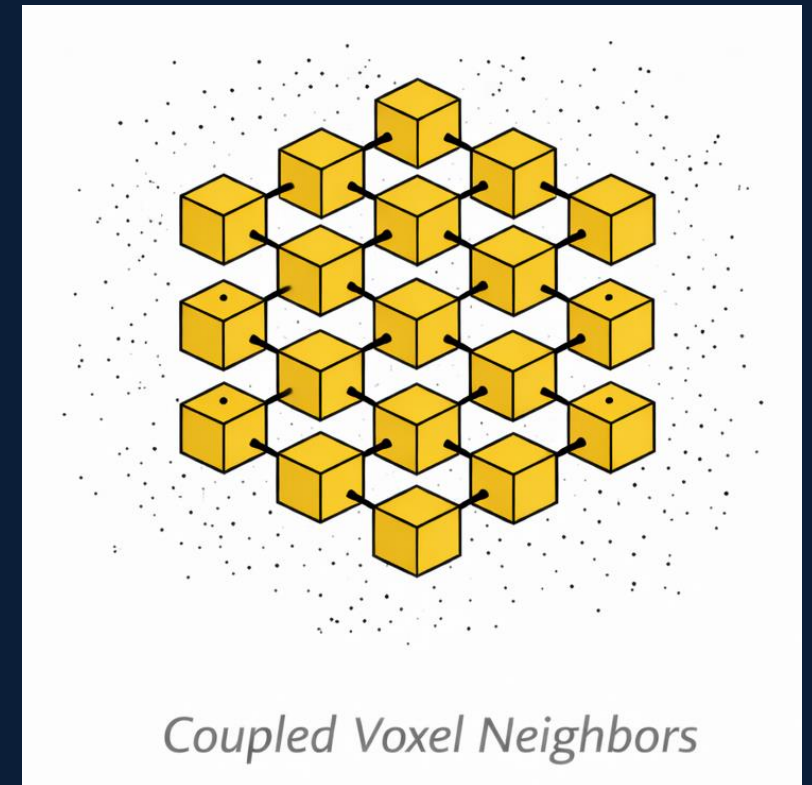
Regularization Framework

Penalized-Likelihood Reconstruction

$$\hat{\mathbf{x}} = \arg \max_{\mathbf{x}} L(\mathbf{y}|\mathbf{x}) - \beta R(\mathbf{x})$$

- Introducing voxel coupling via regularization
- Typically local and handcrafted
- Deep-learning prior may be used

Voxel coupling through regularization



Kernel Representation for Image Reconstruction

- Images are represented by kernels with priors built in:

$$\boldsymbol{x} = \boldsymbol{K}\boldsymbol{\alpha}, \text{ where } \boldsymbol{K} \in \mathbb{R}^{N \times N}$$

- Incorporated into the physics-based forward model

$$\bar{\boldsymbol{y}} = \boldsymbol{P}\boldsymbol{K}\boldsymbol{\alpha} + \boldsymbol{r}$$

- Maximum-likelihood reconstruction: $\hat{\boldsymbol{\alpha}} = \arg \max_{\boldsymbol{\alpha}} L(\boldsymbol{y}|\boldsymbol{K}\boldsymbol{\alpha})$

Kernel Trick for Image Voxels

- Each voxel is a **data sample** with a feature vector $\mathbf{f}_j$
- The voxel intensity is linear in the transformed space:

$$x_j = \mathbf{w}^T \phi(\mathbf{f}_j)$$

- Equivalently, it is described by kernels, which computes **similarity** between voxels

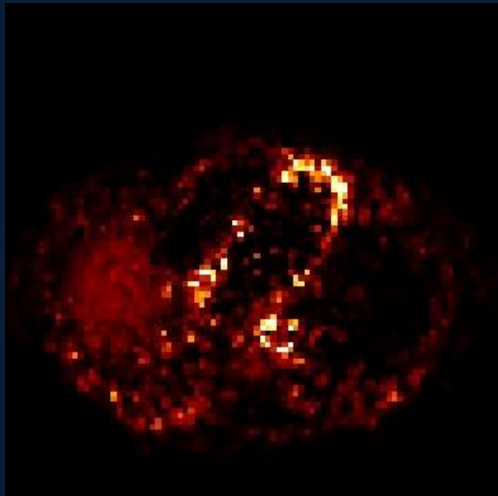
$$x_j = \sum_l \alpha_l \kappa(\mathbf{f}_j, \mathbf{f}_l)$$

where $\kappa(\mathbf{f}_j, \mathbf{f}_l)$ is equal to the inner product of ϕ

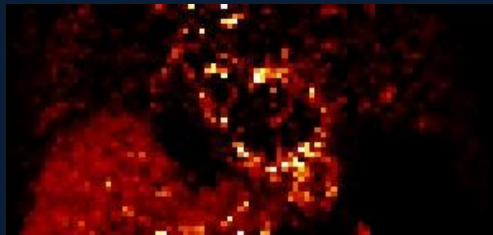
The Kernel Defines Voxel Relational Geometry

- Voxels lie in a non-Euclidean embedding space defined by image priors

3D image from a cardiac scan



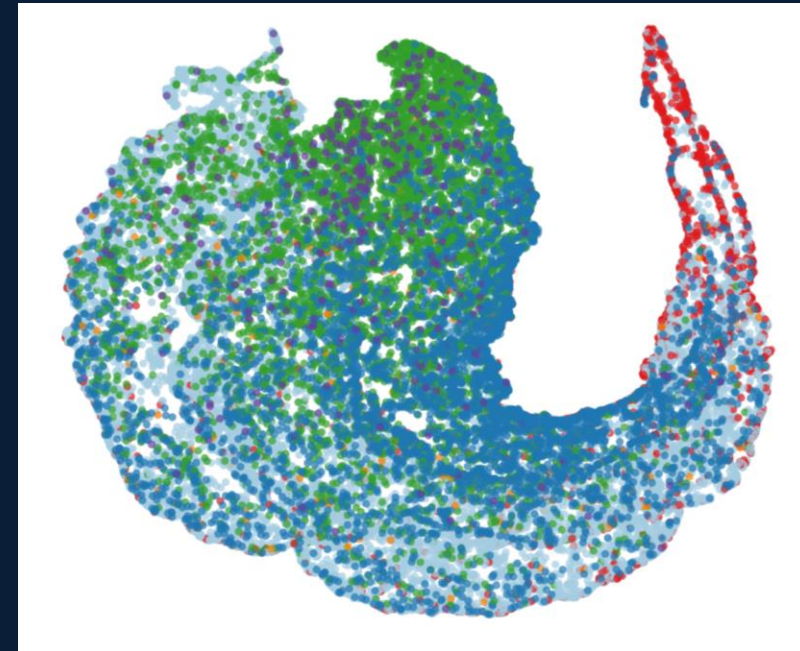
(transverse plane)



(coronal plane)

2D visualization of the voxel embedding

UMAP Embedding 2



UMAP Embedding 1

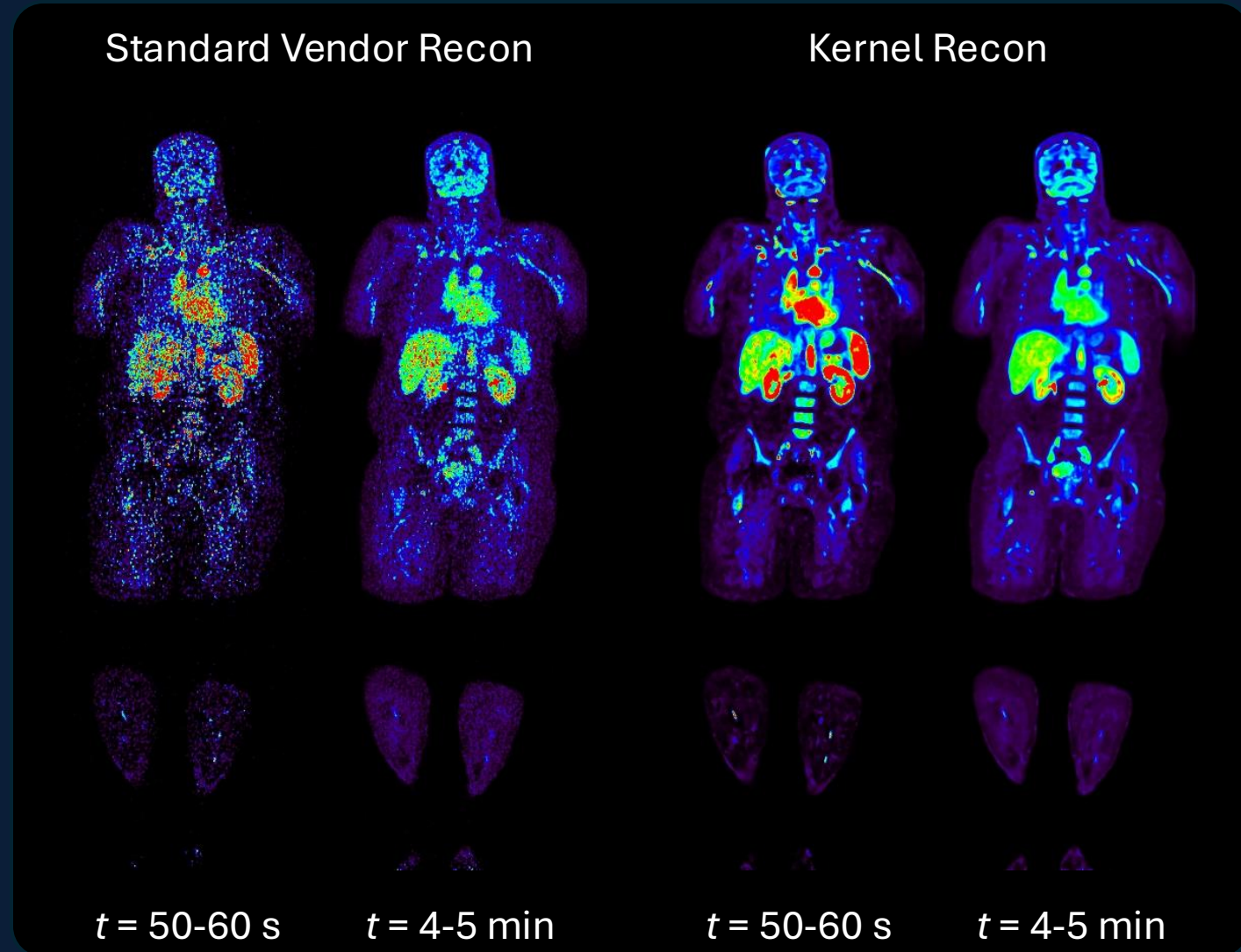


Application to Dynamic PET

- **Image Prior:**
Composite images from longer frames
- **Feature Vector:**
Temporal activity from composite longer frames
- **Reconstruction:**
Dynamic PET images of shorter frames

Wang & Qi 2015; Wang 2019; Zhang *et al* 2020

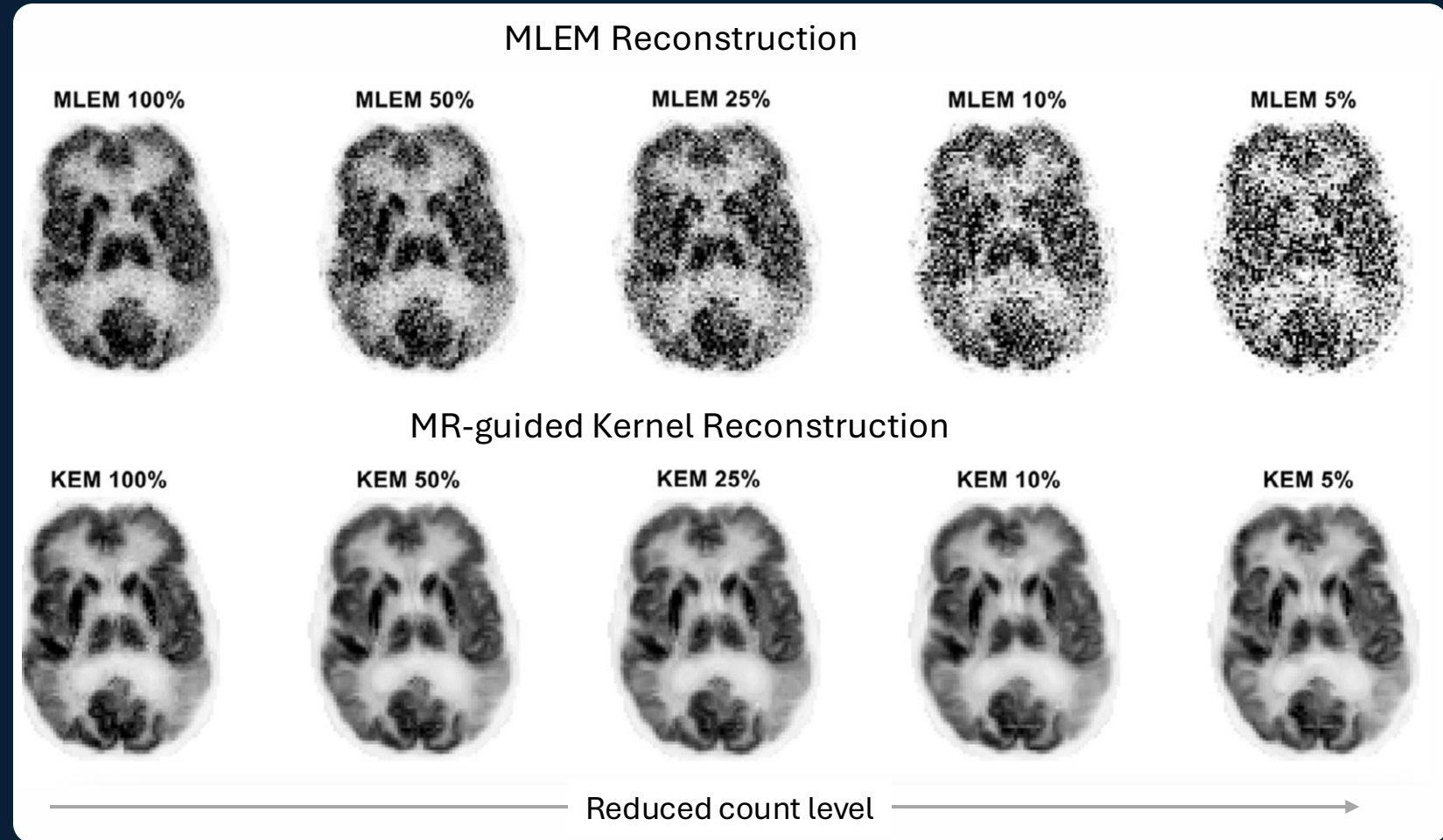
Total-body dynamic FDG-PET Data



PET/MR

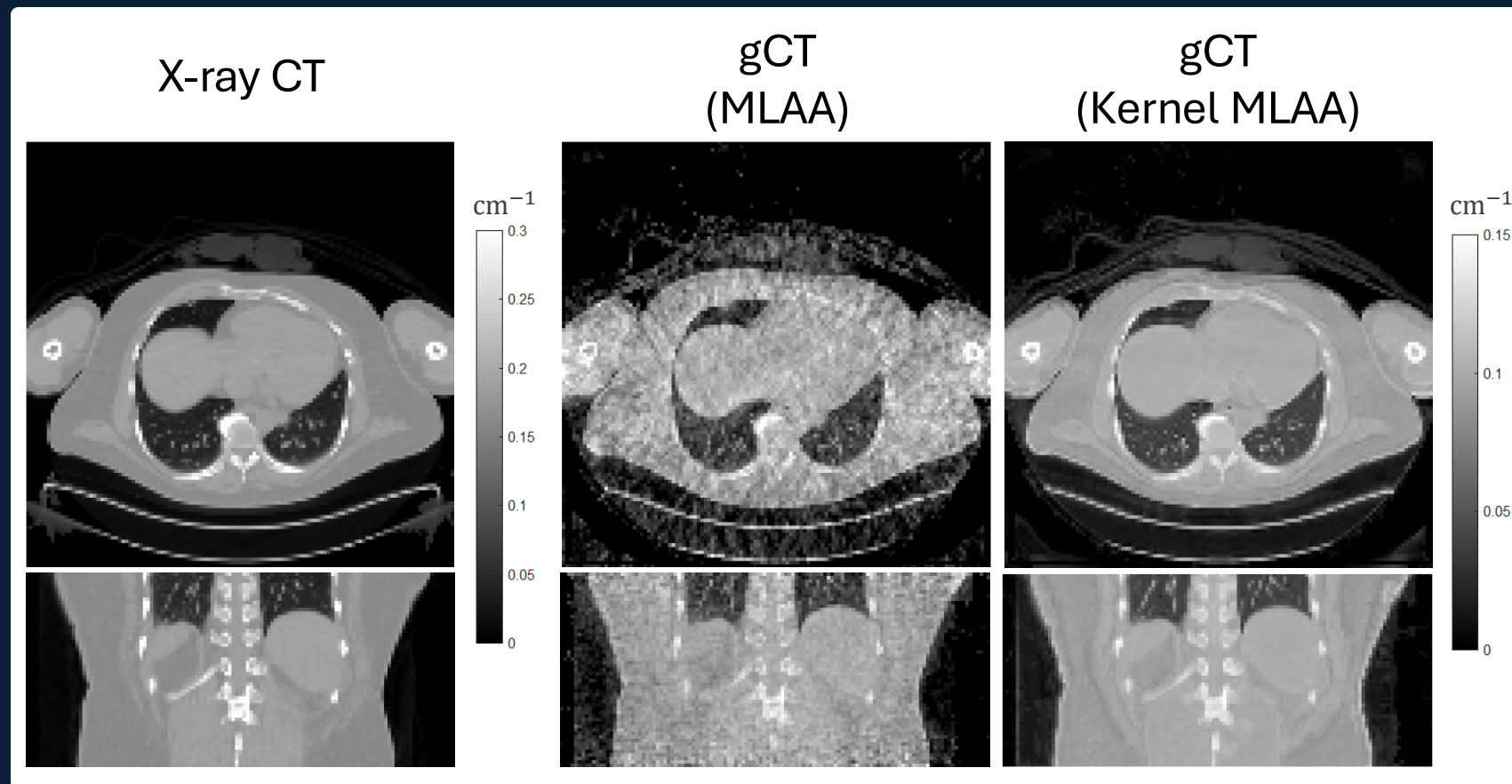
Reader & Pan, BJR 2023

- Image Prior:
MR images
- Feature Vector:
Local MR patch
- Reconstruction:
PET activity image



PET-enabled Dual-Energy CT

- Image Prior:
X-ray CT image
- Feature Vector:
Local CT patch
- Reconstruction:
511 keV gamma-ray
attenuation map (gCT)
from PET emission data



Learning Voxel Representations with Deep Networks

- So far the feature vector is manually designed

f_j = temporal feature or MR patch

- Can we learn the voxel representation?

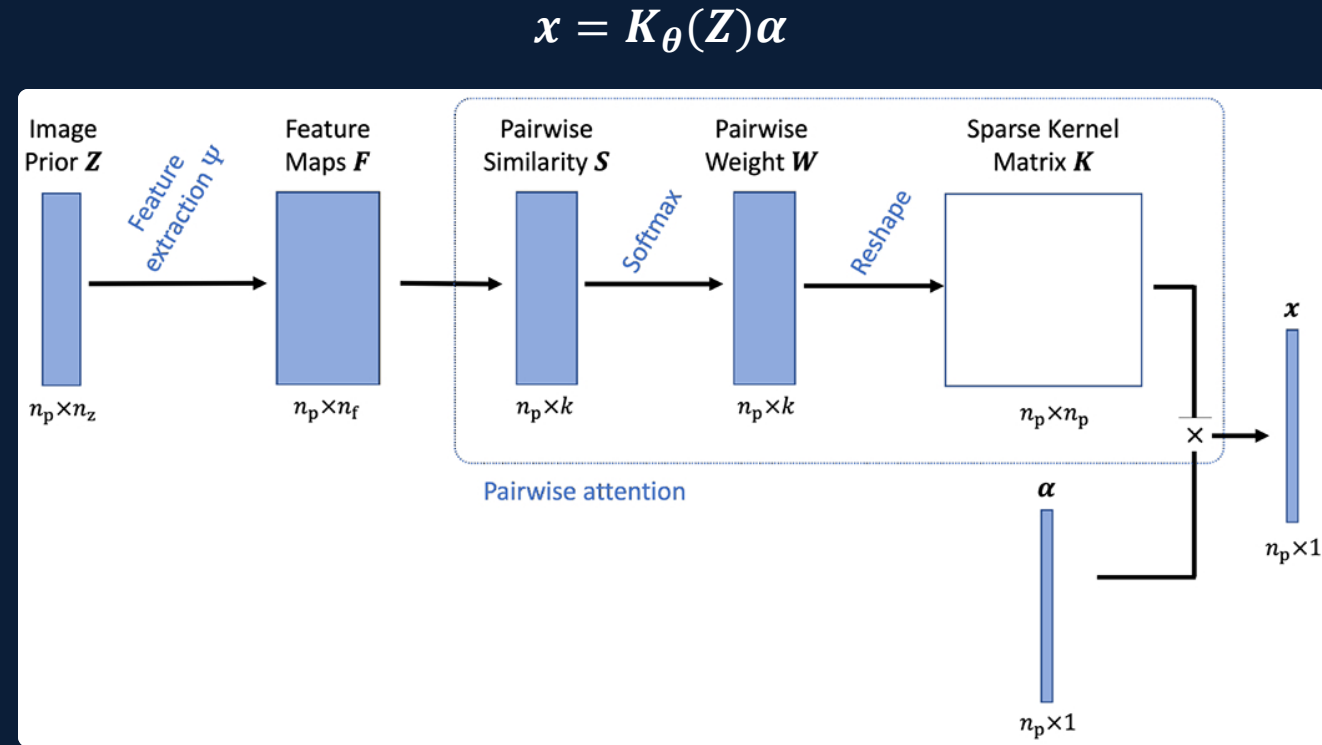


Deep Kernel Representation

- Making kernel construction trainable:

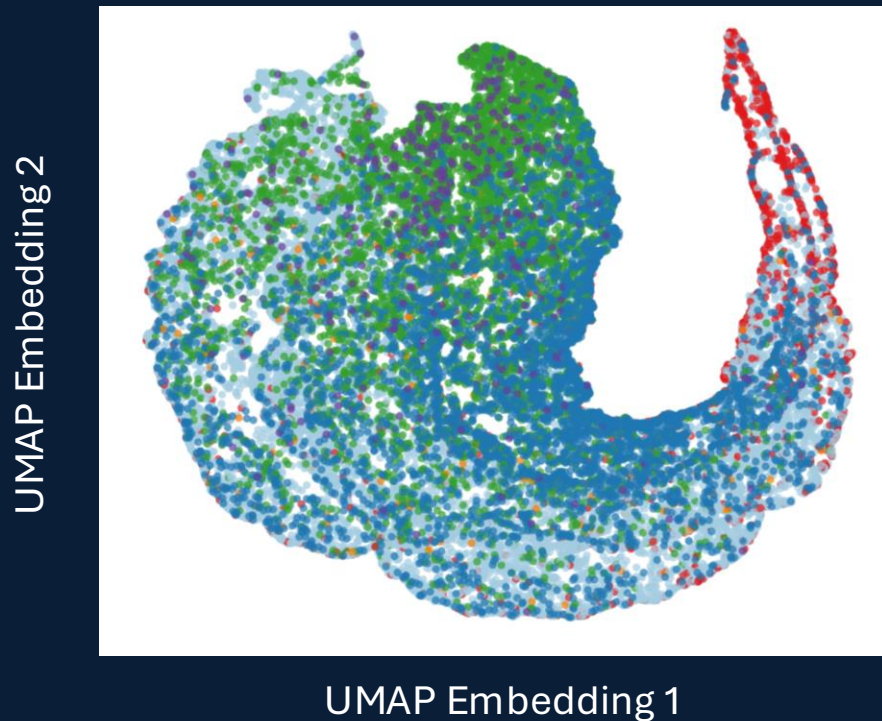
$$x = K_{\theta}(Z)\alpha$$

- **Beauty:** Once θ is determined, the model remains linear w.r.t. α for reconstruction

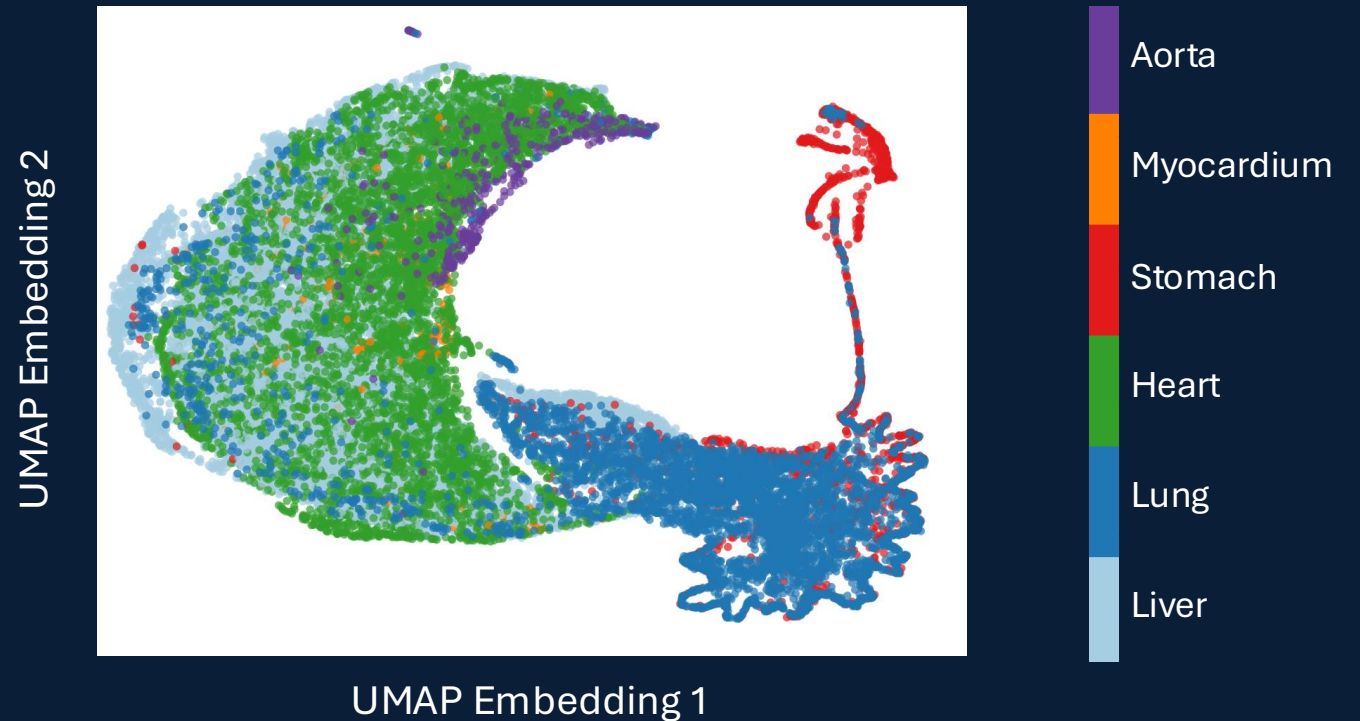


Learned Geometry of Voxel Relations

By handcrafted feature



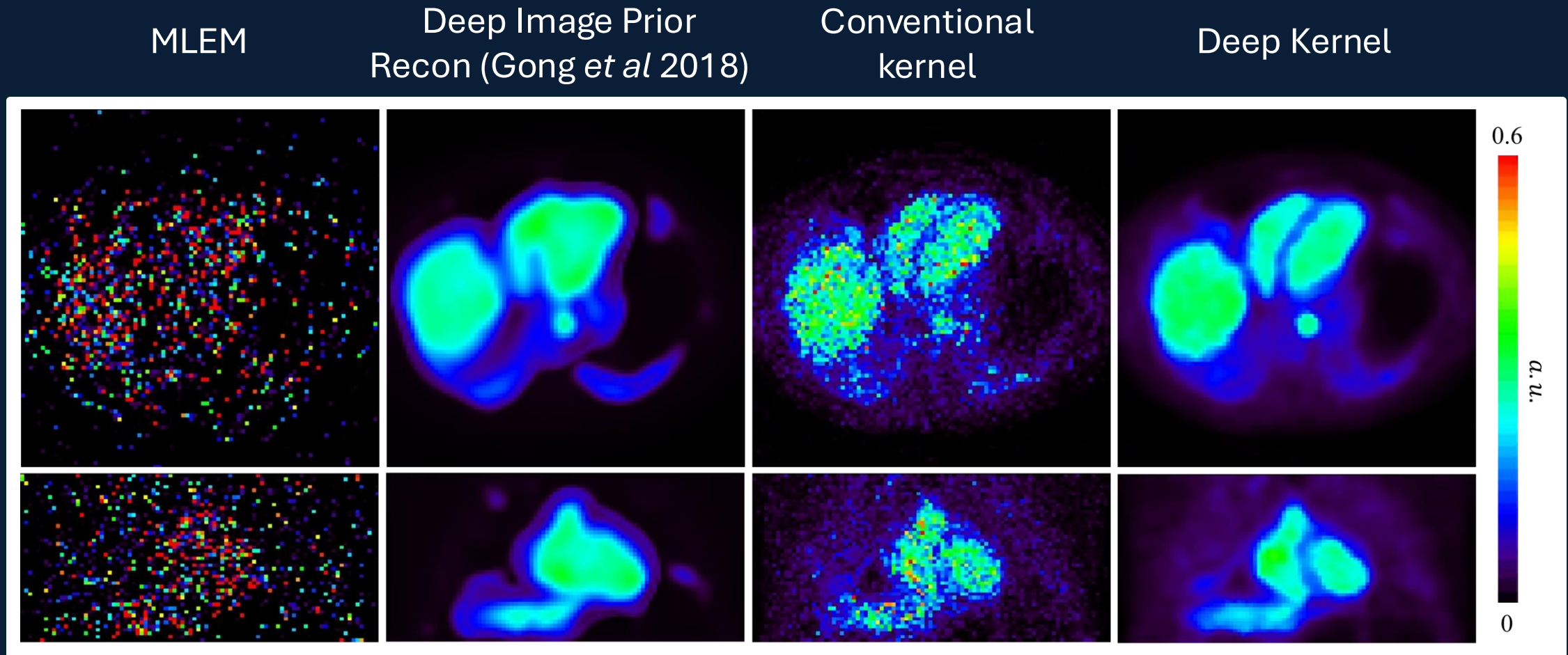
By deep kernel learning



* for a cardiac FDG scan

Reconstruction Example of Patient Data by Deep Kernel

For a 2-s frame in dynamic cardiac FDG-PET imaging:



Limitation of Single-Subject Kernel Learning

Current kernel methods rely on single-subject image prior

Challenges

- Low quality priors may lead to unreliable voxel geometry
- Online kernel learning requires additional time

Pretrained Deep Kernel Construction

Using high- and low-quality image pairs from population data (e.g., generated from total-body PET)

$$\hat{\theta} = \arg \min_{\theta} \sum_n \left\| \mathbf{x}_n^{\text{high}} - \mathbf{K}_{\theta}(\mathbf{x}_n^{\text{low}}) \mathbf{x}_n^{\text{low}} \right\|^2$$

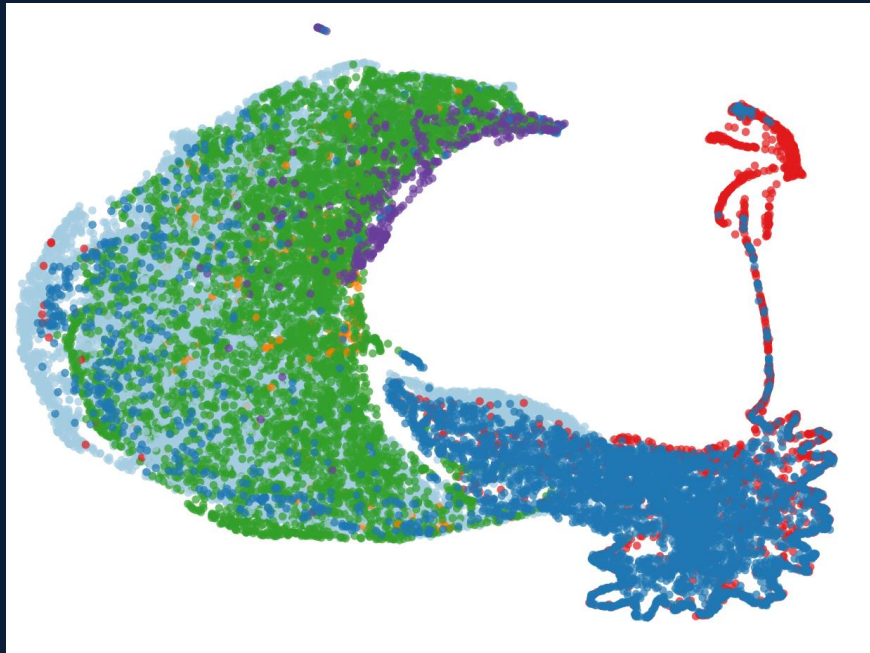
Two important clarifications:

- The network learns how to construct voxel geometry, not the geometry of a particular patient
- Geometry remains subject-specific: $\mathbf{K}_{\theta}(\mathbf{x}^{\text{low}})$

Learned Voxel Geometry by Different Approaches

By single-subject deep kernel

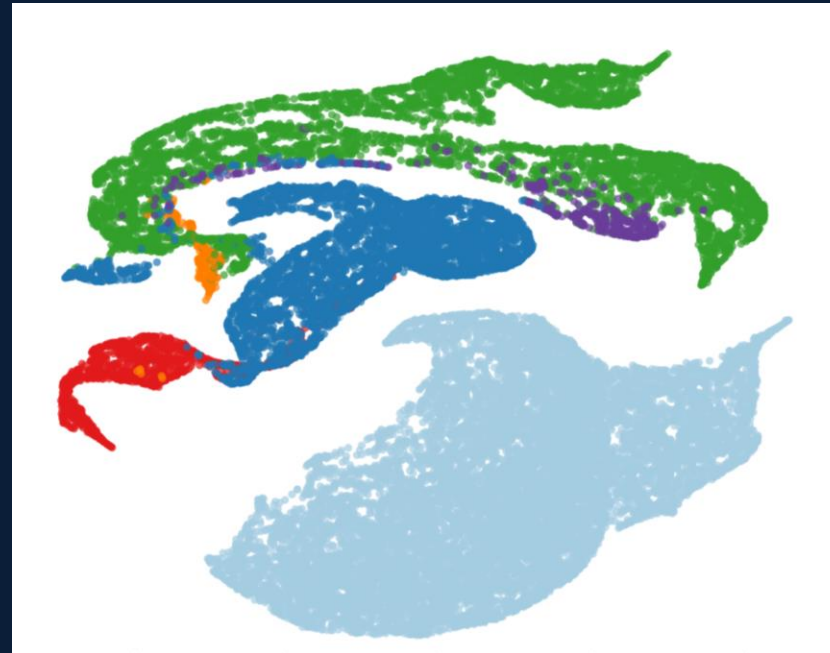
UMAP Embedding 2



UMAP Embedding 1

By pretrained approach

UMAP Embedding 2

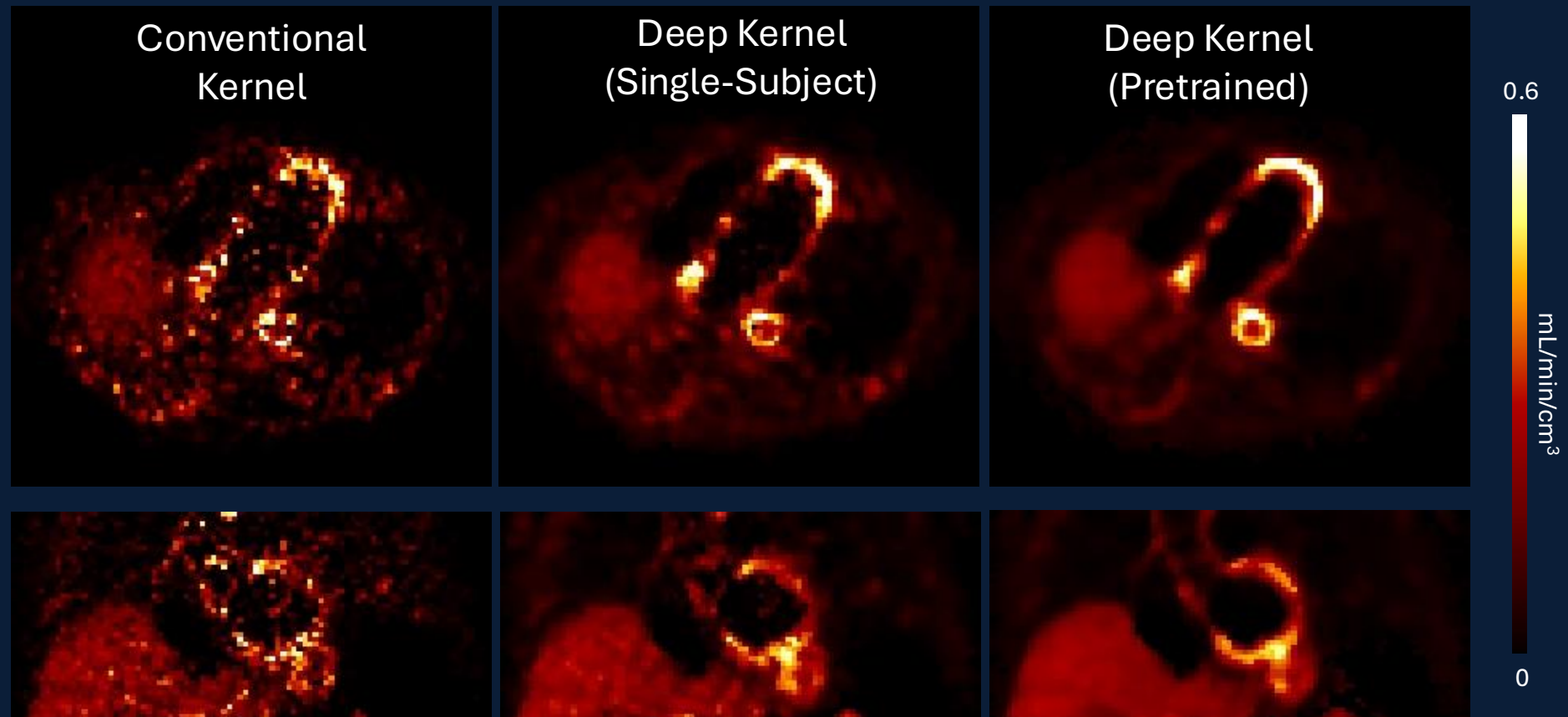


UMAP Embedding 1



Application to Dynamic PET Imaging on Short Scanners

Parametric imaging of FDG delivery rate K_1 from dynamic images reconstructed by different approaches for a GE DST scan



Potential for Static PET Imaging

Dotatate-PET Reference



1/20 low-count OSEM



3D DDPM



Deep Kernel*



*Trained with FDG dataset. Li SQ *et al* IEEE MIC 2025

Closing Thoughts

- Many powerful deep denoisers have been trained for image denoising
- Common use in reconstruction
 - Plug-and-Play
 - Denoising by Regularization (RED)

Can we extract **voxel relational geometry** from deep denoisers?

Thought Experiment

- Taylor expansion of a deep denoiser

$$\mathbf{D}_{\theta}(\mathbf{x}) \approx \mathbf{D}_{\theta}(\mathbf{x}_0) + \mathbf{J}(\mathbf{x}_0)(\mathbf{x} - \mathbf{x}_0)$$

where $\mathbf{J}(\cdot)$ is the Jacobian

- Inspired by the neural tangent kernel (Jacot *et al.*, 2018),

$$\mathbf{K} = \mathbf{J}(\mathbf{x}_0)\mathbf{J}(\mathbf{x}_0)^T$$

may encode voxel relational geometry

Summary

Kernel Reconstruction

= Imaging Physics $\times$ Voxel Relational Geometry

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